

# **AAMI Consensus Report**

# Emergency Use Resuscitator Systems **Design Guidance**

AAMI CR503:2020/(R)2022



*In this redline revision, a vertical line in the margin shows where the technical content is modified from the original.* 

Additions are in green text, deletions are in strikethrough red text.

# Emergency use resuscitator system (EURS) design guidance

Revisions are expected to be made to this document as the COVID-19 situation evolves. Please go to <u>https://www.aami.org/covid\_cr</u> to find the most current version as well as past versions. This document is freely available and may be shared with all interested stakeholders. Contact <u>celliott@aami.org</u> with any comments or questions.

Approved 8 April 2020 and reaffirmed 6 October 2022 by **AAMI** 

**Abstract:** Provides targeted design constraints to enable rapid development of an "ambu bag squeezer" as an emergency use resuscitator system (EURS) to treat patients with COVID-19 respiratory failure. This document is also intended to guide the review of an EURS by an authority having jurisdiction.

Keywords: COVID-19

# **AAMI** Consensus Report

A Consensus Report (CR) is a publication of the Association for the Advancement of Medical Instrumentation (AAMI) developed to provide concise, prompt and practical guidance on narrowly focused topics of high importance to the health technology community. A Consensus Report is intended provide initial consensus guidance in response to an urgent/immediate need for guidance in the following instances:

- While more robust data/information develops on emergent areas
- When variation in the development, implementation or use of a product or process exists
- When existing standards or other documents require additional context/clarification

A Consensus Report is not subject to the same formal process as a standard and while similar in nature to a technical information report (TIR), a CR is based on the collective knowledge and experience of a selected group of stakeholders and has not undergone the wider reviews of a TIR or standard and offers an even greater response time.

**CAUTION NOTICE:** This AAMI CR may be revised or withdrawn at any time. Because it addresses a rapidly evolving field or technology, readers are cautioned to ensure that they have also considered information that may be more recent than this document.

All standards, technical information reports, consensus reports and other types of technical documents developed by AAMI are *voluntary*, and their application is solely within the discretion and professional judgment of the user of the document. Occasionally, voluntary technical documents are adopted by government regulatory agencies or procurement authorities, in which case the adopting agency is responsible for enforcement of its rules and regulations.

Comments on this document are invited and should be sent to AAMI, Attn: Standards Department, 901 N. Glebe Rd, Suite 300, Arlington, VA 22203.

Published by

AAMI 901 N. Glebe Rd., Suite 300 Arlington, VA 22203 www.aami.org

© 2020 by the Association for the Advancement of Medical Instrumentation

#### All Rights Reserved

Publication, reproduction, photocopying, storage, or transmission, electronically or otherwise, of all or any part of this document without the prior written permission of the Association for the Advancement of Medical Instrumentation is strictly prohibited by law. It is illegal under federal law (17 U.S.C. § 101, *et seq.*) to make copies of all or any part of this document (whether internally or externally) without the prior written permission of the Association for the Advancement of Medical Instrumentation. Violators risk legal action, including civil and criminal penalties, and damages of \$100,000 per offense. For permission regarding the use of all or any part of this document, visit the <u>Copyright Clearance Center</u>.

Printed in the United States of America

ISBN 978-1-57020-750-1

# Contents

## Page

Task Group representation	…iv
Acknowledgments	v
Purpose	1
Introduction	1
Review of the requirements of IEC 60601-1 and their applicability to an EURS	3

### **Task Group representation**

#### Association for the Advancement of Medical Instrumentation

#### **COVID-19 Response Team Members**

This AAMI Consensus Report (CR) was developed by a task group under the auspices of the AAMI COVID-19 Response Team.

The AAMI COVID-19 Response Team had the following members:

Cochairs: Jennifer Danieley David Feinstein Julian Goldman Sandy Weininger Members: Simona Bancos, FDA/CDRH Andrew Bath, ResMed Inc. Brandon Blakely, FDA/CDRH Brad Bonnette, ECRI Institute Caitlin Brady, Intertek David Busch, UT Southwestern Medical Center Anthony Ciccarello, Philips Steven Dain. University of Western Ontario Rakhi Dalal, FDA/CDRH Jennifer Danieley, FDA/CDRH Andy Doering, Medtronic Simon Dunham, Weill Cornell Medicine David Feinstein, American Society of Anesthesiologists (ASA) Bruce Friedman, GE Healthcare Hamed Ghods, FDA/CDRH Julian Goldman, Partners HealthCare System Ralf Heesch, Draeger Medical Systems Inc. Heidi Horn, Nuvolo Technologies Fernando Isaza, Philips Michael Jaffe, Cardiorespiratory Consulting LLC Gardner Kimm, Medtronic Inc Campus Robert Kopotic, Edwards Lifesciences Hubertus Lasthaus, VitalAire Germany Ed Madsen, Avanos Medical Phoebe Mainland, Alfred Health Madeleine Manousaridis, Standards Australia Benoit Marchal, Air Liquide Thomas Marmet, GE Healthcare Debra Milamed, Harvard University Cyndy Miller, Medtronic Inc Campus Bryant Moeller, ResMed Inc. Curtis Morgan, 3M Health Care Akito Ohmura, Teikyo University-Mizonokuchi Hospital David Osborn. Philips John Stark, 3M Health Care Robert Steurer, Steurer Consulting Group Dongbo Wang, FDA/CDRH Sandy Weininger, FDA/CDRH

NOTE—Participation by federal agency representatives in the development of this document does not constitute endorsement by the federal government or any of its agencies.

# Acknowledgments

AAMI gratefully acknowledges the writing team members, Julian Goldman, Dave Osborn, Anthony Ciccarello and Sandy Weininger for their outstanding and expeditious work in preparing these drafts for committee review and approval.

# Emergency use resuscitator systems (EURS) design guidance

### 4 Purpose

5 The goals of this document are to provide targeted design constraints to enable rapid development of an 6 "ambu bag squeezer" as an emergency use resuscitator system (EURS) to treat patients with COVID-19 7 respiratory failure. This document is also intended to guide the review of an EURS by an authority having 8 jurisdiction.

9 It is recognized that the surge in COVID-19 is requiring extraordinary measures to provide mechanical 10 ventilatory support to keep pace with clinical need. This global community of clinicians, engineers, 11 manufacturers, regulators, and others are responding to this need by designing and producing, inexpensive, 12 and often open-source, ventilators of varying complexity and capabilities for rapid deployment. This 13 document identifies clinical, engineering and test requirements appropriate to support safe operation. The 14 document identifies requirements that are required for non-EURSs but might not be required for EURSs 15 that have appropriate disclosures. Therefore, equipment complying with the requirements of this document 16 need not provide a level of performance equivalent to that of critical care ventilators (ISO 80601-2-12<sup>1</sup>) or 17 life-supporting homecare ventilators (ISO 80601-2-72<sup>2</sup>) or of ventilatory support equipment (ISO 80601-2-18 80<sup>3</sup>).

19 NOTE This document is intended to be used in conjunction with AAMI CR504:2020, *End user disclosures for* 20 *emergency use resuscitator systems (EURS)*.

### 21 Introduction

The requirements outlined in this paper are modeled on the MIT E-vent<sup>4</sup> ventilator project, where a machine has been designed to replace a trained clinician by mechanically squeezing a user-powered resuscitator (e.g. "ambu bag") as specified in ISO 10651-4<sup>5</sup>.

The requirements outlined in this paper are presuming usage in traditional healthcare facilities (e.g. hospitals, assisted living facilities, nursing homes) as well as spaces converted for the care of large numbers of COVID-19 patients (e.g. convention centers, university dormitories, motels). This paper presumes that the operators of the EURS are all trained professional healthcare providers and not lay

<sup>&</sup>lt;sup>1</sup> ISO 80601-2-12, *Medical electrical equipment* — Part 2-12: Particular requirements for basic safety and essential performance of critical care ventilators

<sup>&</sup>lt;sup>2</sup> ISO 80601-2-72, Medical electrical equipment — Part 2-72: Particular requirements for basic safety and essential performance of home healthcare environment ventilators for ventilator-dependent patients

<sup>&</sup>lt;sup>3</sup> ISO 80601-2-80, *Medical electrical equipment — Part 2-80: Particular requirements for basic safety and* essential performance of ventilatory support equipment for ventilatory insufficiency

<sup>&</sup>lt;sup>4</sup> <u>https://e-vent.mit.edu</u>

<sup>&</sup>lt;sup>5</sup> ISO 10651-4, Lung ventilators — Part 4: Particular requirements for operator-powered resuscitator

29 persons. Hence the requirements of IEC 60601-1<sup>6</sup> specifically the home healthcare environment are 30 considered not applicable to an EURS intended for the treatment of COVID-19 patients.

Fundamentally, the EURS needs to provide ventilation at the patient-connection port as set by the operator or inform the operator via an alarm condition that ventilation is not occurring. Such alarm conditions need to include:

- Electricity supply failure.
- EURS switched off inadvertently.
- Maximum inspiratory airway pressure exceeds 40 cmH<sub>2</sub>O.
- Low inspiratory pressure (equivalent to disconnection alarm condition).
- 38 Continuing pressure
- 39 Estimated tidal volume not achieved or exceeded.
- 40 <u>Note:</u> This equipment is not required to be able to measure tidal volume. For equipment without
   41 the ability to measure tidal volume, it can be estimated e.g., by calibrating the volume delivered
   42 based on the displacement of the resuscitator bag.

The ventilatory support needs of a COVID-19 patient can range from simple BIPAP (bilevel positive airway pressure) for patients that are breathing spontaneously to mandatory ventilation in either a pressure-support or volume control mode. Additionally, these patients are very likely to require inspired oxygen concentrations (FiO<sub>2</sub>) in excess of the 21% contained in room air.

- 47 To properly manage a COVID-19 patient, the EURS needs to indicate to the operator at a minimum:
- The current settings (e.g., inspiratory pressure, tidal volume estimate, frequency).
- The current delivery (e.g., inspiratory pressure, respiratory rate) at the patient-connection port).
- 50 NOTE PEEP is controlled with this equipment by utilizing a PEEP valve attached to the user-powered resuscitator.
- 51 Equipment made according to this specification does not <u>necessarily</u>measure:
- measure flow, so-in which case the tidal volume is not measured. It is only an estimate and is
   dependent on both the patient and model of user-powered resuscitator utilized.
- <u>measure</u> or control FiO<sub>2</sub>. The value of FiO<sub>2</sub> relies on O<sub>2</sub> delivery to the reservoir bag.
- 55 To properly manage a COVID-19 patient, the operator needs to be able to control the EURS at a minimum:
- I:E ratio (ratio of inspiratory to expiratory time) of 1:2 preferably adjustable from 1:1 to 1:4
- Respiratory rate from (10 to 30) inflations/min preferably adjustable in steps of no more than 2 inflations/min

<sup>&</sup>lt;sup>6</sup> IEC 60601-1, Medical electrical equipment — Part 1: General requirements for basic safety and essential performance

- Tidal volume estimate (350 to 450) ml in no more than steps of 50 ml, preferably a lower range of 250 ml and an upper range of 600 ml or 800 ml
- 61 It is recommended that patient monitoring that includes capnography be employed and that continual 62 monitoring of the patient be employed when utilizing an EURS.
- To help prevent contaminating the environment (and particularly the clinicians), filters need to be placed in the expiratory pathways. Particular attention needs to be placed on the exhaust port.

#### 65 Review of the requirements of IEC 60601-1 and their applicability to an EURS

- NOTE 1 Adding an electromechanical squeezing accessory to a non-electrically powered resuscitator complying with
   ISO 10651-4 creates a system that now falls within the scope of IEC 60601-1<sup>7</sup>.
- NOTE 2 Any subclause marked with an asterisk (\*) means that further guidance for this requirement is available in
   Annex A of the standard.
- 70 The GS (the general standard, IEC 60601-1) has required collateral standards (i.e. IEC 60601-1-2<sup>8</sup> on
- EMC, IEC 60601-1-6<sup>9</sup> on usability and IEC 60601-1-8<sup>10</sup> on alarms) that apply to an EURS. There are
- additional applicable collateral standards (and hence requirements) if the EURS is intended for home use,
- 73 ambulance use or as part of a physiological closed loop control system. These standards can be purchased
- from many sources including ANSI<sup>11</sup> and AAMI<sup>12</sup>.
- NOTE 3 Words written in small caps are not 'normal English'. They are defined terms and have specific, defined
   meanings. See Clause 3 in the GS for their definitions.

#### 77 Clause 3 Terminology and definitions

78 Additional definitions include:

#### 79 AIRWAY PRESSURE

- 80 pressure at the PATIENT-CONNECTION PORT, relative to ambient pressure unless otherwise specified
- Note 1 to entry: In addition to its direct reference, this term or its symbol  $P_{aw}$ , displayed in various character styles, is only used, in context or by qualification, to designate this concept as a measured quantity.
- Note 2 to entry: The site(s) of actual measurement(s) may be anywhere in the breathing system, providing that the indicated value is referenced to that at the PATIENT-CONNECTION PORT.
- Note 3 to entry: This is the generic term for this fundamental concept. Post-coordinated terms, for example, peak inspiratory pressure and baseline airway pressure, are used in particular contexts.

<sup>&</sup>lt;sup>7</sup> IEC 60601-1, *Medical electrical equipment* — *Part 1: General requirements for basic safety and essential performance* 

<sup>&</sup>lt;sup>8</sup> IEC 60601-1-2, Medical electrical equipment — Part 1-2: General requirements for basic safety and essential performance - Collateral Standard: Electromagnetic disturbances - Requirements and tests

<sup>&</sup>lt;sup>9</sup> IEC 60601-1-6, Medical electrical equipment — Part 1-6: General requirements for basic safety and essential performance - Collateral standard: Usability

<sup>&</sup>lt;sup>10</sup> IEC 60601-1-8, Medical electrical equipment — Part 1-8: General requirements for basic safety and essential performance - Collateral Standard: General requirements, tests and guidance for alarm systems in medical electrical equipment and medical electrical systems

<sup>&</sup>lt;sup>11</sup> ANSI, https://webstore.ansi.org/

<sup>&</sup>lt;sup>12</sup> AAMI, https://my.aami.org/store/

- 87 Note 4 to entry: Although providing no explicit indication as to where along the PATIENT'S airway this pressure is
- 88 measured, this term, along with its symbol, has become widely adopted as referencing the pressure at the point at
- 89 which artificial-ventilation equipment is connected to the PATIENT'S airway or to an airway device. This is the final site 90 where a common and replicable pressure can be continuously monitored, conveniently, before breathing gas enters
- 90 where a common an 91 the PATIENT.
- 92 Note 5 to entry: A pressure measured in the PATIENT'S airway at a site other than at the PATIENT-CONNECTION PORT is 93 referred to in this document as a respiratory pressure.

#### 94 **BIOCOMPATIBILITY**

- ability to be in contact with a living system without producing an unacceptable adverse effect
- 96 Note 1 to entry: Medical devices may produce some level of adverse effect, but that level may be determined to be 97 acceptable when considering the benefits provided by the medical device.

#### 98 GAS PATHWAY

- 99 interior surfaces, over which gases or liquids that can be inspired, in a medical device bounded by the ports
- 100 through which gases or liquids enter and leave the medical device including the patient interface or the
- 101 interior surfaces of enclosures that are in contact with gases or liquids that can be inspired
- 102 Note 1 to entry: PATIENT contact surfaces such as the outer surfaces of a tracheal tube or the cushion of a mask are 103 evaluated according to the ISO 10993 series.
- 104 EXAMPLE 1 The breathing system, inlet filter, gas mixer, blower and internal piping.
- 105 EXAMPLE 2 Enclosed chamber of an incubator including the mattress or the inner surface of an oxygen hood.
- 106 EXAMPLE 3 The inner surfaces of breathing tubes, tracheal tubes or masks and mouthpieces.

#### 107 MONITORING EQUIPMENT

108 ME EQUIPMENT or part that continuously or continually measures and indicates the value of a variable to the 109 OPERATOR

#### 110 PATIENT-CONNECTION PORT

- 111 port of a breathing system intended for connection to an airway device
- 112 Note 1 to entry: The PATIENT-CONNECTION PORT is the end of the ventilator breathing system proximal to the patient.
- 113 Note 2 to entry: The PATIENT-CONNECTION port is typically in the form of a suitable for connection to an airway device 114 such as a tracheal or tracheostomy tube, a face mask, or a supralaryngeal airway, or to a test apparatus.
- 115 Note 3 to entry: Current particular standards typically specify that the PATIENT-CONNECTION PORT is required to be in the 116 form of a specific standardized connector(s), for example, a connector(s) conforming to ISO 5356-1.
- 117 Note 4 to entry: In ventilators designed to provide NIV (non-invasive ventilation) and where the ventilation function is
- dependent upon a design feature of a component that connects the ventilator to the *patient's* airway, then the PATIENT-
- 119 CONNECTION PORT typically becomes the contact line of the seal to the PATIENT'S face and there is no PATIENT-CONNECTION
- 120 PORT connector.

#### 121 PROTECTION DEVICE

part or function of ME EQUIPMENT that, without intervention by the OPERATOR, protects the PATIENT from
 hazardous output due to incorrect delivery of energy or substances

#### 124 Clause 5 General requirements for testing of ME EQUIPMENT

125 This Clause of the GS is fully required.

#### 126 Clause 6 Classification of ME EQUIPMENT and ME SYSTEMS

- 127 This Clause of the GS is fully required.
- 128 An EURS may be Class I or Class II or internally powered.

129 Unless there are electrical connections to the PATIENT (e.g. monitoring ACCESSORIES) or heated breathing

130 tubes or electrically powered ACCESSORIES (e.g. expiratory valves located proximal to the PATIENT), the

- 131 plastic breathing tubes provide adequate floating electrical isolation.
- Protection from the ingress of water: IP21 should be required and IP22 is recommended for the electricalparts. Body fluids and IV bags are an expected normal part of the environment of use.
- 134 Since the EURS compresses a resuscitator that can contain an oxygen concentration in excess of the 25 %,
- the considerations for an OXYGEN RICH ENVIRONMENT apply (see IEC 60601-1, 11.2.2). However, if care has
- been taken to ensure that any motor and the electronics are not in the oxygen rich environment, then these
- 137 requirements do not apply.

#### 138 Clause 7 ME EQUIPMENT identification, marking and documents

#### 139 7.1 General

- 140 This subclause of the GS is recommended but not required.
- 141 Rationale: Although ensuring that the EURS can be read both over the indicated illumination level and the
- 142 indicated cone of visibility is recommended, in this pandemic situation it is not considered mandatory. It is
- 143 noted that operators are likely wearing PPE and will have reduced visual acuity. Consideration should be
- 144 given to doubling the distance of the observer.

#### 145 **7.2** Marking on the outside of ME EQUIPMENT or ME EQUIPMENT parts

146 This subclause of the GS is required.

#### 147 7.3 Marking on the inside of ME EQUIPMENT OF ME EQUIPMENT parts

148 This subclause of the GS is required.

#### 149 **7.4** Marking of controls and instruments

150 This subclause of the GS is required.

#### 151 **201.7.4.2 Control devices**

- 152 This subclause is required.
- 153 **201.7.4.3 Units of measurement**
- 154 This subclause is required.
- 155 7.5 Safety signs
- 156 This subclause of the GS is required.

#### 157 **7.6 Symbols**

- 158 This subclause of the GS is required.
- 159 7.7 Colours of the insulation of conductors
- 160 This subclause of the GS is required.
- 161 **7.8 Indicator lights and controls**
- 162 This subclause of the GS is required.
- 163 NOTE The pending amendment to the GS clarifies this requirement.

#### 164 7.9 ACCOMPANYING DOCUMENTS

165 This subclause of the GS is required.

#### 166 201.7.9.1 Additional general requirements

167 This subclause is required.

#### 168 Clause 8 Protection against electrical HAZARDS from ME EQUIPMENT

169 This Clause of the GS is generally required.

NOTE 1 Unless there are electrical connections to the PATIENT (e.g. monitoring ACCESSORIES) or heated breathing tubes
 or electrically powered ACCESSORIES (e.g. expiratory valves located proximal to the patient), the plastic breathing tubes
 provide adequate floating electrical isolation for PATIENT LEAKAGE CURRENT.

NOTE 2 Commercially available ITC (information technology communications) power supplies can be used, but
 electrical safety criteria (e.g. ENCLOSURE TOUCH CURRENTS and dielectric withstand) are likely to exceed IEC 60601-1
 limits. This can be mitigated in several ways such as:

- Use of a low leakage SEPARATION DEVICE (isolation transformer) (see 16.5 of the GS);
- A second PERMANENTLY INSTALLED PROTECTIVE EARTH CONNECTION (see 16.6 of the GS);
- Instructing the OPERATOR to not touch the EURS and the PATIENT at the same time.

#### 179 Clause 9 Protection against MECHANICAL HAZARDS of ME EQUIPMENT and ME SYSTEMS

- 180 This Clause of the GS is recommended but not required, except for 9.2 and 9.3 that are required.
- 181 Clause 10 Protection against unwanted and excessive radiation HAZARDS
- 182 This Clause of the GS is required.
- 183 Clause 11 Protection against excessive temperatures and other HAZARDS
- 184 This Clause of the GS is required, except as indicated below.
- 185 **11.7 BIOCOMPATIBILITY OF ME EQUIPMENT and ME SYSTEMS**
- 186 The GAS PATHWAYS should be evaluated for BIOCOMPATIBILITY according to ISO 18562-1:2017.

187 The chosen materials for the GAS PATHWAYS need to be reasonably pure and simple in nature (minimize the 188 use of additives where possible). Avoid Polyvinyl chloride (PVC) in the GAS PATHWAYS. When possible, 189 efforts should be taken to use materials which have a long history of safe use in currently marketed medical 190 devices. Care is needed to ensure that gas pathways are free of foreign material (e.g. oil, particles, volatile 191 organic compounds, mold release agents should be avoided in the GAS PATHWAYS). Care is needed to 192 ensure that GAS PATHWAYS do not contain toxic compounds (e.g., formaldehyde), and do not release noxious 193 gases (e.g., ozone, carbon monoxide) and fumes. The ACCOMPANYING DOCUMENTS should include 194 cautionary statement for any BIOCOMPATIBILITY identified RISK.

Rationale: The tests of ISO 18562 (series)<sup>13</sup> are very expensive, time consuming to perform and require very specialized test equipment. Requiring these tests for an EURS would so delay their availability such that new designs would not be available when needed. The preponderance of the gas pathways (i.e. the user-powered resuscitator and tubing) are existing legally marketed medical devices.

#### 199 **11.8** Interruption of the power supply/supply mains to ME EQUIPMENT

- 200 This subclause is required with the following additions:
- a) An EURS shall be equipped with an INTERNAL ELECTRICAL POWER SOURCE.
- b) An EURS shall be equipped with an automatic switchover to the internal electrical power source
   when the supply mains falls outside the values necessary to maintain normal operation.
- 204 c) A fully charged INTERNAL ELECTRICAL POWER SOURCE shall be capable of powering the EURS for at
   205 least 30 min.
- 206 d) A means shall be provided for determining the state of this INTERNAL ELECTRICAL POWER SOURCE.
- 207 e) A means shall be provided to indicate that the EURS is powered from the INTERNAL ELECTRICAL
   208 POWER SOURCE.
- 209 f) The EURS shall either:
- 210 1) be equipped with an ALARM SYSTEM that:
- 211i)detects an ALARM CONDITION of at least a LOW PRIORITY to indicate the switchover to the212INTERNAL ELECTRICAL POWER SOURCE;
- 213ii)detects an ALARM CONDITION of at least a MEDIUM PRIORITY to indicate that the INTERNAL214ELECTRICAL POWER SOURCE is nearing depletion at least 15 min prior to the loss of215ventilation;
- 216
   2) or be equipped with an INTELLIGENT ALARM SYSTEM, based on additional information, determines
   217
   218
   218
   219
   210
   210
   211
   211
   211
   212
   213
   213
   213
   214
   215
   216
   217
   218
   218
   218
   218
   218
   218
   210
   211
   211
   211
   211
   212
   213
   213
   214
   215
   215
   216
   217
   218
   218
   218
   218
   218
   218
   218
   218
   218
   218
   218
   218
   218
   218
   218
   219
   210
   210
   211
   211
   211
   211
   212
   213
   214
   215
   215
   216
   217
   218
   218
   218
   218
   218
   218
   218
   218
   218
   218
   218
   218
   218
   218
   218
   218
   218
   218
   218
   218
   218
   218
   219
   210
   210
   210
   211
   211
   211
   211
   211
   211
   211
   211
   211
   211
   211
   211
   211
   211
   211
   211
   211
   211
   211
   211
   211
   211
- NOTE The OPERATOR needs sufficient time "prior to the loss of all power" to take action to ensure that alternative arrangements can be made to continue the function of the EURS.
- 221 g) The instructions for use shall disclose:

<sup>&</sup>lt;sup>13</sup> ISO 18562 (series), *Biocompatibility evaluation of breathing gas pathways in healthcare applications* 

222 223	1)	the operational time of the EURS when powered from each power source under the following conditions a fully charged power source and the conditions of Table 201.102;
224	2)	the behavior of the EURS after a switch-over to:
225		i) the INTERNAL ELECTRICAL POWER SOURCE, or
226		ii) an alternative SUPPLY MAINS.
227	3)	the behavior of the EURS while the recharging of:
228		i) the INTERNAL ELECTRICAL POWER SOURCE, or
229		ii) an alternative SUPPLY MAINS.
230	4)	the minimum time between complete loss of INTERNAL ELECTRICAL POWER SOURCE, and
231 232		i) the start of the LOW PRIORITY impending INTERNAL ELECTRICAL POWER SOURCE failure ALARM CONDITION, and
233 234		ii) the MEDIUM PRIORITY impending INTERNAL ELECTRICAL POWER SOURCE failure alarm condition.

- 235 Check conformance by functional testing and inspection of the instructions for use.
- An external UPS (uninterruptable power supply) may be used to fulfill this requirement.

Rationale: The power back up and appropriate notification of power loss is what is important. It need notbe integrated into the EURS.

#### 239 Clause 12 Accuracy of controls and instruments and protection against hazardous outputs

240 This Clause of the GS is required, except as indicated below.

#### 241 **124.2** Usability of ME EQUIPMENT

242 Conformance with IEC 60601-1-6 is recommended, but not required.

Rationale: USABILITY as described in IEC 60601-1-6 ensures safety by proscribing a design PROCESS. A
 proper USABILITY evaluation is extremely time consuming and requires subject matter experts. A hard to use
 EURS can be better than no EURS.

#### 246 **124.3** ALARM SYSTEMS

247 Conformance with IEC 60601-1-8 is recommended, but not required.

Rationale: Full conformance with IEC 60601-1-8 would be helpful to the OPERATORS as they would more readily understand the operation of the EURS ALARM SYSTEM. Care needs to be taken with auditory ALARM SIGNALS to ensure that they are not too obtrusive, appropriately priority encoded (so that more urgent problems are more highlighted) and there must be a means to inactivate any auditory ALARM SIGNAL. The ALARM SYSTEM, ALARM LIMITS, and ALARM CONDITION priorities are complex areas to optimize for USABILITY.

Annex A of IEC 60601-1-8 provides a great deal of guidance.

#### 254 12.4 Protection against hazardous output

- 255 Additional requirements:
- 256 12.4.101 Measurement of AIRWAY PRESSURE
- 257 12.4.101.1 General
- 258 a) The EURS shall be equipped with MONITORING EQUIPMENT to indicate the AIRWAY PRESSURE.
- b) The site of actual measurement may be anywhere in the breathing system, but the indicated valueshall be referenced to the PATIENT-CONNECTION PORT.
- 261 c) Under steady-state conditions, the indicated AIRWAY PRESSURE shall be accurate to within 262  $\pm (2 + 4 \% \text{ of the actual reading}) \text{ hPa (cmH}_2\text{O}).$
- 263 d) The EURS should indicate the plateau pressure at end inspiration, if measured.

NOTE This is measured by holding the user-powered resuscitator bag compressed at the end of inspiration for approximately 200 ms allowing the plateau pressure to be measured.

- 266 Check conformance by functional testing.
- 267 12.4.101.2 LOW AIRWAY PRESSURE ALARM CONDITION
- a) The AIRWAY PRESSURE MONITORING EQUIPMENT shall be equipped with an ALARM SYSTEM that detects
   an ALARM CONDITION to indicate when the low AIRWAY PRESSURE ALARM LIMIT is reached.
- 270 b) The low AIRWAY PRESSURE ALARM CONDITION:
- 271 1) shall be at least a MEDIUM PRIORITY, unless
- 272 2) an INTELLIGENT ALARM SYSTEM, based on additional information, determines that:
- 273 i) the low AIRWAY PRESSURE ALARM CONDITION is suppressed, or
- ii) its priority is changed, or
- 275 3) may start at LOW PRIORITY, and
- 276 4) if this state continues, escalate to medium priority.
- 277 c) The low AIRWAY PRESSURE ALARM SIGNAL may be inactivated with ALARM OFF.
- d) ALARM OFF may be activated by the EURS.
- e) The low AIRWAY PRESSURE ALARM LIMIT may be:
- 280 1) pre-adjusted,
- 281 2) RESPONSIBLE ORGANIZATION-adjustable,
- 282 3) OPERATOR-adjustable,
- 283 4) EURS-adjustable, or

284	5) a combination of operator-adjustable and EURS-adjustable.
285 286	f) If the airway pressure alarm limit is adjustable by the EURS, a summary description of the algorithm that determines the alarm limit value shall be disclosed in the instructions for use.
287	NOTE Depending on the type of ventilation mode being utilized, there can be more than one active ALARM LIMIT.
288	Check conformance by functional testing.
289 290 291	<ul> <li>12.4.101.3 High-pressure ALARM CONDITION and PROTECTION DEVICE         <ul> <li>a) The EURS shall be equipped with an ALARM SYSTEM that detects a high AIRWAY PRESSURE ALARM CONDITION to indicate when the high AIRWAY PRESSURE ALARM LIMIT is reached.</li> </ul> </li> </ul>
292	b) The high AIRWAY PRESSURE ALARM CONDITION:
293	1) shall be HIGH PRIORITY, unless
294	2) an INTELLIGENT ALARM SYSTEM, based on additional information, determines that
295	i) the high AIRWAY PRESSURE ALARM CONDITION is suppressed, or
296	ii) its priority is changed.
297	c) The high AIRWAY PRESSURE ALARM LIMIT may be:
298	1) independently adjustable,
299	2) connected to an adjustable pressure limitation, or
300	3) related to the set pressure of the EURS.
301 302	d) If the high AIRWAY PRESSURE ALARM LIMIT is independently adjustable, it shall not be possible to set the ALARM LIMIT to a value greater than <u>640 hPa (40 cmH<sub>2</sub>O)</u> .
303 304 305	d)e)Means shall be provided to require the OPERATOR to perform a deliberate sequence of actions to confirm the setting of the adjustable high –AIRWAY PRESSURE ALARM LIMIT to values exceeding 40 cmH <sub>2</sub> O.
306 307	<del>o)</del> <u>f</u> )_PATIENT-generated transient pressure increases should not cause the high AIRWAY PRESSURE ALARM CONDITION.
308	EXAMPLE Transient pressure increase caused by the patient coughing.
309 310	f)g) The high AIRWAY PRESSURE ALARM CONDITION DELAY shall not exceed 200 ms and the EURS shall arrest the pressure rise.
311	Check conformance by functional testing.
	12.4.102 Continuing pressure ALARM CONDITION
312	
312 313 314	a) The EURS shall be equipped with an ALARM SYSTEM that detects a continuing positive pressure of less than 10 cmH <sub>2</sub> O variation longer than 15 s.

316	1) shall be HIGH PRIORITY, unless
317	2) an INTELLIGENT ALARM SYSTEM, based on additional information, determines that
318	i) the continuing positive pressure ALARM CONDITION is suppressed, or
319	ii) its priority is changed.
320	Check conformance compliance by functional testing.
321	12.4.103 Estimated tidal volume ALARM CONDITIONS
322 323	Note: If the EURS is equipped with flow measurement, tidal volume can be measured and used instead of an estimated value for this subclause.
324 325	a) The EURS shall be equipped with an ALARM SYSTEM that detects a deviation in estimated tidal volume of more than 20 %.
326	b) The low estimated tidal volume ALARM CONDITION:
327	1) shall be MEDIUM PRIORITY, unless
328	2) an INTELLIGENT ALARM SYSTEM, based on additional information, determines that:
329	i) the low estimated tidal volume ALARM CONDITION is suppressed, or
330	ii) its priority is changed.
331	c) The high estimated tidal volume ALARM CONDITION:
332	1) shall be MEDIUM PRIORITY, unless
333	2) an INTELLIGENT ALARM SYSTEM, based on additional information, determines that
334	i) the high estimated tidal volume ALARM CONDITION is suppressed, or
335	ii) its priority is changed.
336	12.4.104 Protection against inadvertent setting of high AIRWAY PRESSURE
337 338	Means shall be provided to require the <i>operator</i> to perform a deliberate sequence of actions to confirm any airway pressure settings exceeding 40 cmH <sub>2</sub> O.
339	Check conformance compliance by functional testing.
340	Clause 13 HAZARDOUS SITUATIONS and fault conditions for ME EQUIPMENT
341	This Clause of the GS is required with following addition:
342	Independence of ventilation control function and related RISK CONTROL measures
343	a) A SINGLE FAULT CONDITION shall not cause the simultaneous failure of:
344	1) the ventilation-control function; and
345	2) the corresponding PROTECTION DEVICE.

- b) A SINGLE FAULT CONDITION shall not cause failure in such a way that a failure of:
- the ventilation-control function and the corresponding MONITORING EQUIPMENT is not detected,
   or
- 349 2) the ventilation-control function and the corresponding ALARM SYSTEM is not detected.
- 350 Check conformance by inspection and functional testing.
- 351 Clause 14 PROGRAMMABLE ELECTRICAL MEDICAL SYSTEMS (PEMS)
- 352 This Clause of the GS is recommended but not required.
- 353 Clause 15 Construction of ME EQUIPMENT
- 354 This Clause of the GS is required.
- 355 Additional requirements:

#### 356 15.3.101 Mechanical strength

The EURS shall be tested with each user-powered resuscitator indicated in the instructions for use at the maximum tidal volume and breath rate setting for a minimum of 24 h.

359 Check conformance by functional testing and inspection of the user-powered resuscitator to confirm that 360 the user-powered resuscitator has not been damaged, that the breathing system remains connected and 361 that the user-powered resuscitator remains in place.

362 Additional requirement:

#### 363 15.3.102 Mechanical strength

The user-powered resuscitator shall remain positioned in the EURS when oxygen tubing (connected to the oxygen tube nipple) is pulled with a force of  $(40 \pm 5)$  N at any angle within a cone of 45° to the major axis of the user-powered resuscitator.

367 Check conformance with the following test:

368 Attach oxygen tubing connector to the oxygen tube nipple using axial hand pressure and a twisting motion.

369 Position the user-powered resuscitator in the EURS according to the instructions for use. Smoothly pull the

370 oxygen tubing away from the user-powered resuscitator with a force of (40 ±5) N at any angle within a cone

- 371 of 45° to the major axis of the user-powered resuscitator.
- 372 Confirm that the user-powered resuscitator remains in place and is ready to use. Disconnection of the 373 oxygen tubing connector from the oxygen tube nipple is not considered a failure.
- 374 Clause 16 ME systems
- 375 This Clause of the GS is required.

#### 376 Clause 17 Electromagnetic compatibility of ME EQUIPMENT and ME SYSTEMS

377 This Clause is recommended but not required.

Rationale: The tests of IEC 60601-1-2 are time consuming and expensive set of tests that take very specialized equipment. Requiring these tests for an EURS would delay availability such that new designs might not be available when needed. Disclosure that these tests have not been performed and that other equipment must be kept at a distance should be considered sufficient.

382 Additional requirements for an EURS:

#### 383 Spontaneous breathing during loss of power supply

- a) A PROTECTION DEVICE shall be provided to allow spontaneous breathing when normal ventilation is
   compromised as a result of the electrical or pneumatic supply power being outside the values
   necessary for normal operation.
- b) The PROTECTION DEVICE may be provided by a MASK or ACCESSORY.
- 388 c) Under these conditions, the inspiratory and expiratory pressure drop measured at the PATIENT 389 CONNECTION PORT with all recommended ACCESSORIES in place shall not exceed
   390 6,0 hPa (6,0 cmH<sub>2</sub>O) at a flowrate of:
- 391 1) 30 l/min for EURS intended to provide a DELIVERED VOLUME,  $V_{del} \ge 300 \text{ ml}$ ;
- 392 2) 15 l/min for EURS intended to provide a DELIVERED VOLUME,  $V_{del} \le 300$  ml;
- 393 NOTE This requirement is intended to allow the patient to breathe spontaneously under compromised conditions.

394 Check conformance by functional testing and measurement of flowrate, pressure, and resistance at the 395 patient-connection port with that combination of accessories indicated in the instructions for use which 396 produces the greatest pressure drop.

#### 397 Training

- In the application of the requirements of IEC 62366-1:2015<sup>14</sup>, 5.6, 5.7.1 b), 5.7.3 d) and 5.8 training shall be considered necessary for both the OPERATOR and the designee of the RESPONSIBLE ORGANIZATION.
- 400 NOTE Requirements for training are found in IEC 62366-1:2015, 5.8.
- 401 Check conformance by inspection of the ACCOMPANYING DOCUMENT and the USABILITY ENGINEERING FILE.

#### 402 **POWER SUPPLY CORDS**

- Any DETACHABLE POWER SUPPLY CORD or detachable d.c. power cord of an electrically powered EURS shall be protected against accidental disconnection from the EURS under a force of 30 N.
- 405 Check conformance by inspection and, for EURS when provided with an APPLIANCE COUPLER or detachable 406 d.c. power cord, by the following test.
- 407 a) Subject the DETACHABLE POWER SUPPLY CORD for 1 min to an axial pull of force of 30 N.
- b) During the test, the MAINS CONNECTOR becoming disconnected from the APPLIANCE INLET or the detachable d.c. power cord becoming disconnected from the d.c. input connector of the EURS is considered a failure.

<sup>&</sup>lt;sup>14</sup> IEC 62366-1:2015, Medical devices - Part 1: Application of usability engineering to medical devices